

# Package ‘dcmriS4’

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**Title** A Package for Medical Image Analysis (S4 implementation)

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**Depends** R (>= 2.14.0), oro.nifti (>= 0.3.9)

**Suggests** bitops, minpack.lm, splines, XML, oro.dicom (>= 0.3.7)

**Imports** grDevices, graphics, methods, parallel, utils

**Description** A collection of routines and documentation that allows one to perform voxel-wise quantitative analysis of dynamic contrast-enhanced or diffusion-weighted MRI data, with emphasis on oncology applications.

**License** BSD\_3\_clause + file LICENSE

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**R topics documented:**

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dcmriS4-package	<i>dcmri: A Package for Medical Image Analysis (S4 implementation)</i>
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**Description**

A collection of routines and documentation that allows one to perform a quantitative analysis of dynamic contrast-enhanced or diffusion-weighted MRI data. Medical imaging data should be organized using either the Analyze or NIfTI data formats.

**Details**

Package: dcmriS4  
Version: 0.20.1  
Date: 2009-09-02  
Depends: R (>= 2.6.0), grDevices, graphics, methods, utils  
Suggests: bitops, minpack.lm, multicore, splines, XML  
License: BSD  
URL: <http://www.dcmri.org/>, <http://dcmri.sourceforge.net/>

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Further information is available in the following vignettes:

dcmriS4 dcmriS4(source, pdf)

### Author(s)

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Maintainer: Brandon Whitcher <bjw34032@users.sourceforge.net>

### References

Schmid, V., Whitcher, B., Padhani, A.R., Taylor, N.J. and Yang, G.-Z. (2006) Bayesian methods for pharmacokinetic models in dynamic contrast-enhanced magnetic resonance imaging, *IEEE Transactions on Medical Imaging*, **25** (12), 1627-1636.

Schmid, V., Whitcher, B., Padhani, A.R. and G.-Z. Yang (2009) A semi-parametric technique for the quantitative analysis of dynamic contrast-enhanced MR images based on Bayesian P-splines, *IEEE Transactions on Medical Imaging*, **28** (6), 789-798.

### Examples

```
## Not run:
demo(avg152T1)
demo(avg152T1LR)
demo(avg152T1RL)
demo(buckley)
demo("filtered_func_data")
demo(zstat1)

## End(Not run)
```

---

aifParameters      *Parameters for Arterial Input Functions*

---

**Description**

Specification of parameters for arterial input functions (AIFs)

**Usage**

```
aifParameters(type, user = NULL)
```

**Arguments**

`type`            is one of the following character strings associated with an AIF:

- `tofts.kermode`
- `fritz.hansen`
- `orton.exp`
- `orton.cos`
- `user`
- `empirical`

`user`            is a vector of estimated AIF parameters or the empirical AIF values.

**Details**

...

**Value**

...

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>

**See Also**

[compartmentalModel](#), [dcmri.lm](#)

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 Apparent Diffusion Coefficient

*Estimate the Apparent Diffusion Coefficient (ADC)*

---

**Description**

Estimation of apparent diffusion coefficient (ADC) values, using a single exponential function, is achieved through nonlinear optimization.

**Usage**

```
adc.lm(signal, b, guess, control=minpack.lm::nls.lm.control())
## S4 method for signature 'array'
ADC.fast(dwi, bvalues, dwi.mask,
         control=minpack.lm::nls.lm.control(maxiter=150),
         multicore=FALSE, verbose=FALSE)
```

**Arguments**

signal	Signal intensity vector as a function of b-values.
b, bvalues	Diffusion weightings (b-values).
guess	Initial values of $S_0$ and $D$ .
control	An optional list of control settings for <code>nls.lm</code> . See <code>nls.lm.control</code> for the names of the settable control values and their effect.
dwi	Multidimensional array of diffusion-weighted images.
dwi.mask	Logical array that defines the voxels to be analyzed.
multicore	is a logical variable (default = FALSE) that allows parallel processing via <b>multicore</b> .
verbose	Additional information will be printed when <code>verbose=TRUE</code> .

**Details**

The `adc.lm` function estimates parameters for a vector of observed MR signal intensities using the following relationship

$$S(b) = S_0 \exp(-bD),$$

where  $S_0$  is the baseline signal intensity and  $D$  is the apparent diffusion coefficient (ADC). It requires the routine `nls.lm` that applies the Levenberg-Marquardt algorithm. Note, low b-values (< 50 or < 100 depending on who you read) should be avoided in the parameter estimation because they do not represent information about the diffusion of water in tissue.

The `ADC.fast` function rearranges the assumed multidimensional (2D or 3D) structure of the DWI data into a single matrix to take advantage of internal R functions instead of loops, and called `adc.lm`.

**Value**

A list structure is produced with estimates of  $S_0$ ,  $D$  and information about the convergence of the nonlinear optimization routine.

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>

**References**

Buxton, R.B. (2002) *Introduction to Functional Magnetic Resonance Imaging: Principles & Techniques*, Cambridge University Press: Cambridge, UK.

Callahan, P.T. (2006) *Principles of Nuclear Magnetic Resonance Microscopy*, Clarendon Press: Oxford, UK.

Koh, D.-M. and Collins, D.J. (2007) Diffusion-Weighted MRI in the Body: Applications and Challenges in Oncology, *American Journal of Roentgenology*, **188**, 1622-1635.

**See Also**

[nls.lm](#)

**Examples**

```
S0 <- 10
b <- c(0, 50, 400, 800) # units?
D <- 0.7e-3             # mm^2 / sec (normal white matter)

## Signal intensities based on the (simplified) Bloch-Torrey equation
dwi <- function(S0, b, D) {
  S0 * exp(-b*D)
}

set.seed(1234)
signal <- array(dwi(S0, b, D) + rnorm(length(b), sd=0.15),
               c(rep(1,3), length(b)))
ADC <- ADC.fast(signal, b, array(TRUE, rep(1,3)))
unlist(ADC) # text output

par(mfrow=c(1,1)) # graphical output
plot(b, signal, xlab="b-value", ylab="Signal intensity")
lines(seq(0,800,10), dwi(S0, seq(0,800,10), D), lwd=2, col=1)
lines(seq(0,800,10), dwi(ADC$S0, seq(0,800,10), ADC$D), lwd=2, col=2)
legend("topright", c("True", "Estimated"), lwd=2, col=1:2)
```

---

 Arterial Input Functions

*Arterial Input Functions*


---

**Description**

Parametric models for arterial input functions (AIFs) that are compatible with single compartment models for dynamic contrast-enhanced MRI (DCE-MRI).

**Usage**

```
aif.orton.exp(tt, AB, muB, AG, muG)
model.orton.exp(tt, aparams, kparams)
orton.exp.lm(tt, aif, guess=c(log(100),log(10),log(1),log(0.1)),
             nprint=0)
```

**Arguments**

<code>tt</code>	is a vector of acquisition times (in minutes) relative to injection of the contrast agent. Negative values should be used prior to the injection.
<code>AB, muB, AG, muG</code>	are parameters of the double exponential function that describe the AIF.
<code>aparams</code>	is the vector of parameters ( $A_B, \mu_B, A_G, \mu_G$ ) associated with the AIF.
<code>kparams</code>	is the vector of parameters ( $v_p, K^{trans}, k_{ep}$ ) associated with the “extended Kety model” for contrast agent concentration.
<code>aif</code>	is the vector of observed contrast agent concentrations (data) used to estimate the parametric model.
<code>guess</code>	Initial parameter values for the nonlinear optimization.
<code>nprint</code>	is an integer, that enables controlled printing of iterates if it is positive. In this case, estimates of par are printed at the beginning of the first iteration and every <code>nprint</code> iterations thereafter and immediately prior to return. If <code>nprint</code> is not positive, no tracing information on the progress of the optimization is produced.

**Details**

`aif.orton.exp` displays the exponential AIF from Orton *et al.* (2008) for a known set of AIF parameter values. `model.orton.exp` displays the exponential AIF from Orton *et al.* (2008) for a known set of AIF and compartmental model parameter values. `orton.exp.lm` estimates the AIF parameters, using nonlinear optimization, using a vector of observed contrast agent concentrations.

**Value**

`aif.orton.exp` and `model.orton.exp` return the AIF associated with the pre-specified parameter values.

`orton.exp.lm` returns a list structure with

`AB`                    The amplitude of the first exponential function.



muB	The decay rate of the first exponential function.
AG	The amplitude of the second exponential function.
muG	The decay rate of the second exponential function.
info	The success (or failure) code from the Levenburg-Marquardt algorithm <code>nls.lm</code> .
message	The text message associated with the <code>info</code> parameters.

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>

**References**

Orton, M.R., Collins, D.J., Walker-Samuel, S., d'Arcy, J.A., Hawkes, D.J., Atkinson, D. and Leach, M.O. (2007) Bayesian estimation of pharmacokinetic parameters for DCE-MRI with a robust treatment of enhancement onset time, *Physics in Medicine and Biology* **52**, 2393-2408.

Orton, M.R., d'Arcy, J.A., Walker-Samuel, S., Hawkes, D.J., Atkinson, D., Collins, D.J. and Leach, M.O. (2008) Computationally efficient vascular input function models for quantitative kinetic modelling using DCE-MRI, *Physics in Medicine and Biology* **53**, 1225-1239.

**See Also**

[dcmri.lm](#), [extract.aif](#), [nls.lm](#)

**Examples**

```
data("buckley")
## Generate AIF params using the orton.exp function from Buckley's AIF
xi <- seq(5, 300, by=5)
time <- buckley$time.min[xi]
aif <- buckley$input[xi]
aifparams <- orton.exp.lm(time, aif)
aifparams$D <- 1
unlist(aifparams[1:4])

aoe <- aif.orton.exp(time, aifparams$AB, aifparams$muB, aifparams$AG,
                   aifparams$muG)
with(buckley, plot(time.min, input, type="l", lwd=2))
lines(time, aoe, lwd=2, col=2)
legend("right", c("Buckley's AIF", "Our approximation"), lty=1,
       lwd=2, col=1:2)
cbind(time, aif, aoe)[1:10,]
```

---

Buckley

*Simulated Data from Buckley (2002)*

---

### Description

In Buckley (2002) tissue residue curves for a Meningioma and a Breast Cancer were simulated using the MMID4 model. Note, the model is described in detail by Bassingthwaighe, J.B. *et al.* (1984) and Kroll, K *et al.* (1996). This model accounts for flow dispersion and heterogeneity, and includes capillaries modeled as axially distributed blood-tissue exchange units. A plasma concentration-time curve, AKA arterial input function, was simulated as an input to the model using measurements made by Fritz-Hansen *et al.* (1996).

### Usage

```
data("buckley")
```

### Format

Two lists are created (breast and meningioma) that contain the simulated time curves and all associated kinetic parameter values.

### Source

See below.

### References

- Buckley, D.L. (2002) Uncertainty in the Analysis of Tracer Kinetics Using Dynamic Contrast-Enhanced  $T_1$ -weighted MRI, *Magnetic Resonance in Medicine* **47**, 601-606.
- Bassingthwaighe, J.B. and Goresky, C.A. (1984) Modelling in the analysis of solute and water exchange in the microvasculature. In: Renkin, E.M., Michel, C.C. and Geiger, S.R., editors. Handbook of physiology. Section 2. The cardiovascular system. Bethesda: American Physiological Society. p549-626.
- Kroll, K., Wilke, N., Jerosch-Herold, M., Wang, Y., Zhang Y., Basche, R.J. and Bassingthwaighe, J.B. (1996) Modelling regional myocardial flows from residue functions of an intravascular indicator. *Am J Physiol* **271**, H1643-H1655.
- Fritz-Hansen, T., Rostrup, E., Larsson, H.B., Sondergaard, L., Ring, P. and Hendriksen, O. (1996) Measurement of the arterial concentration Gd-DTPA using MRI; a step toward quantitative perfusion imaging. *Magn Reson Med* **36**, 347-357.

---

 compartmentalModel      *Compartmental Models for Kinetic Parameter Estimation*


---

### Description

A selection of parametric models are provided that combine a compartmental model for tissue and a functional form of the arterial input function.

### Usage

compartmentalModel(type)

### Arguments

type	is a character string that identifies the type of compartmental model to be used. Acceptable models include: <b>“weinmann”</b> Weinmann AIF convolved with a single compartment (Kety) model <b>“extended”</b> Kety model extended with additional vascular compartment (default) <b>“orton.exp”</b> Extended model using Orton’s exponential arterial input function <b>“orton.cos”</b> Extended model using Orton’s raised cosine arterial input function <b>“kety.orton.exp”</b> Kety model using Orton’s exponential arterial input function <b>“kety.orton.cos”</b> Kety model using Orton’s raised cosine arterial input function <b>“weinmann.empirical”</b> User-specified empirical AIF convolved with a single compartment model <b>“extended.empirical”</b> Extended model using a user-specified empirical arterial input function
------	--

### Details

Parametric models from the DCE-MRI literature are provided to the user for kinetic parameter estimation. All models, with the exception of those marked ‘empirical’ incorporate a parametric model for the arterial input function (AIF).

### Value

A function.

### Author(s)

Brandon Whitcher <bjw34032@users.sourceforge.net>

### See Also

[aifParameters](#), [dcmri.bayes](#), [dcmri.lm](#), [dcmri.map](#)

---

`conv.fft`*Convolution of 3D Arrays using the Fourier Transform*

---

**Description**

Convolve a

**Usage**

```
conv.fft(A, B, C, FFTA=NULL)
```

**Arguments**

A	is a three-dimensional array (“the template”).
B	is a three-dimensional array (“the target”).
C	is a vector of length three (the center of “the template”).
FFTA	is the three-dimensional Fourier transform of A, this may save time when looping over multiple “targets”.

**Details**

The arrays *A* and *B* are transformed into the Fourier domain and multiplied together (equivalent to a convolution in the image domain across all spatial locations simultaneously).

**Value**

A three-dimensional array, the same dimension as the input arrays, that is the convolution of the “target” to the “template” at all spatial locations.

**Author(s)**

Brandon Whitcher

**References**

Briggs, W.L. and Henson, V.E. (1995) *The DFT: An Owner’s Manual for the Discrete Fourier Transform*, SIAM: Philadelphia.

**See Also**

[fft](#), [ftm](#), [shift3D](#)

**Examples**

```

cube <- array(0, c(20,20,1))
cube[9:12,9:12,1] <- 1
tkernel <- array(0, c(20,20,1))
tkernel[,,1] <- c(.5, 1, .5, rep(0,20-3))
tcenter <- find.center(iffelse(tkernel > 0, TRUE, FALSE))
out <- conv.fft(tkernel, cube, tcenter)
out[8:13,8:13,1] ## text output

par(mfrow=c(2,2)) ## graphic output
image(drop(tkernel), col=tim.colors(), main="Template")
image(drop(cube), col=tim.colors(), main="Target")
image(drop(out), col=tim.colors(), main="Output")

```

CPMG

*Quantitative T2***Description**

...

**Usage**

```

T2.lm(signal, TE, guess, control=minpack.lm::nls.lm.control())
## S4 method for signature 'array'
T2.fast(cpmg, cpmg.mask, TE,
        control=minpack.lm::nls.lm.control(maxiter=150),
        multicore=FALSE, verbose=FALSE)

```

**Arguments**

signal	is the vector of signal intensities as a function of echo times.
TE	is the vector of echo times (in seconds).
guess	is the vector of initial values for the parameters of interest: $\rho$ and $T2$ .
control	An optional list of control settings for <code>nls.lm</code> . See <code>nls.lm.control</code> for the names of the settable control values and their effect.
cpmg	is a multidimensional array of signal intensities. The last dimension is assumed to be a function of the echo times, while the previous dimensions are assumed to be spatial.
cpmg.mask	is a (logical) multidimensional array that identifies the voxels to be analyzed.
multicore	is a logical variable (default = FALSE) that allows parallel processing via <b>multi-core</b> .
verbose	is a logical variable (default = FALSE) that allows text-based feedback during execution of the function.

**Details**

...

**Value**

A list structure is produced with (all or some of the) parameter estimates

$\rho$	Scaling factor between signal intensity and T2 (proton density).
T2	T2 relaxation time.

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>

**See Also**

[R1.fast](#), [R10.1m](#)

**Examples**

```
## Example?
```

---

 dam

*Double-Angle Method for B1+ Mapping*

---

**Description**

For in vivo MRI at high field ( $\geq 3$  T) it is essential to consider the homogeneity of the active B1 field (B1+). The B1+ field is the transverse, circularly polarized component of B1 that is rotating in the same sense as the magnetization. When exciting or manipulating large collections of spins, nonuniformity in B1+ results in nonuniform treatment of spins. This leads to spatially varying image signal and image contrast and to difficulty in image interpretation and image-based quantification.

**Usage**

```
dam(low, high, low.deg)
```

**Arguments**

low	is the (3D) array of signal intensities at the low flip angle.
high	is the (3D) array of signal intensities at the high flip angle (note, $2*\text{low} = \text{high}$ ).
low.deg	is the low flip angle (in degrees).

## Details

The proposed method uses an adaptation of the double angle method (DAM). Such methods allow calculation of a flip-angle map, which is an indirect measure of the B1+ field. Two images are acquired:  $I_1$  with prescribed tip  $\alpha_1$  and  $I_2$  with prescribed tip  $\alpha_2 = 2\alpha_1$ . All other signal-affecting sequence parameters are kept constant. For each voxel, the ratio of magnitude images satisfies

$$\frac{I_2(r)}{I_1(r)} = \frac{\sin \alpha_2(r) f_2(T_1, TR)}{\sin \alpha_1(r) f_1(T_1, TR)}$$

where  $r$  represents spatial position and  $\alpha_1(r)$  and  $\alpha_2(r)$  are tip angles that vary with the spatially varying B1+ field. If the effects of  $T_1$  and  $T_2$  relaxation can be neglected, then the actual tip angles as a function of spatial position satisfy

$$\alpha(r) = \arccos \left( \left| \frac{I_2(r)}{2I_1(r)} \right| \right)$$

A long repetition time ( $TR \leq 5T_1$ ) is typically used with the double-angle methods so that there is no  $T_1$  dependence in either  $I_1$  or  $I_2$  (i.e.,  $f_1(T_1, TR) = f_2(T_1, TR) = 1.0$ ). Instead, the proposed method includes a magnetization-reset sequence after each data acquisition with the goal of putting the spin population in the same state regardless of whether the  $\alpha_1$  or  $\alpha_2$  excitation was used for the preceding acquisition (i.e.,  $f_1(T_1, TR) = f_2(T_1, TR) \neq 1.0$ ).

## Value

An array, the same dimension as the acquired signal intensities, is returned containing the multiplicative factor associated with the low flip angle acquisition. That is, if no B1+ inhomogeneity was present then the array would only contain ones. Numbers other than one indicate the extent of the inhomogeneity as a function of spatial location.

## Author(s)

Brandon Whitcher <<bjw34032@users.sourceforge.net>>

## References

Cunningham, C.H., Pauly, J.M. and Nayak, K.S. (2006) Saturated Double-Angle Method for Rapid B1+ Mapping, *Magnetic Resonance in Medicine*, **55**, 1326-1333.

---

dcmri.bayes

*Bayesian Methods for Pharmacokinetic Modeling of Dynamic Contrast-Enhanced MRI Data*

---

## Description

Bayesian analysis of contrast agent concentration time curves from DCE-MRI.

**Usage**

```
## S4 method for signature 'array'
dcmri.bayes(conc, time, img.mask, model="extended",
            aif=NULL, user=NULL, nriters=3000, thin=3, burnin=1000,
            tune=267, ab.ktrans=c(0,1), ab.kep=ab.ktrans,
            ab.vp=c(1,19), ab.tauepsilon=c(1,1/1000),
            samples=FALSE, multicore=FALSE, verbose=FALSE, dic=FALSE,
            ...)
dcmri.bayes.single(conc, time, nriters=3000, thin=3,
                  burnin=1000, tune=267, ab.gamma=c(0,1),
                  ab.theta=c(0,1), ab.vp=c(1,19),
                  ab.tauepsilon=c(1,1/1000), aif.model=0,
                  aif.parameter=c(2.4,0.62,3,0.016), vp=1)
```

**Arguments**

conc	Matrix or array of concentration time series (last dimension must be time).
time	Time in minutes.
img.mask	Mask matrix or array. Voxels with mask=0 will be excluded.
model	is a character string that identifies the type of compartmental model to be used. Acceptable models include: <ul style="list-style-type: none"> <li>• “weinmann”Tofts &amp; Kermode AIF convolved with single compartment model</li> <li>• “extended”Weinmann model extended with additional vascular compartment (default)</li> <li>• “orton.exp”Extended model using Orton’s exponential AIF</li> <li>• “kety.orton.exp”Kety model using Orton’s exponential AIF</li> </ul>
aif	is a character string that identifies the parameters of the type of arterial input function (AIF) used with the above model. Acceptable values are: tofts.kermode (default) or fritz.hansen for the weinmann and extended models; orton.exp (default) or user for the orton.exp and kety.orton.exp model.
user	Vector of AIF parameters. For Tofts and Kermode: $a_1, m_1, a_2, m_2$ ; for Orton <i>et al.</i> : $A_b, \mu_b, A_g, \mu_g$ .
nriters	Total number of iterations.
thin	Thinning factor.
burnin	Number of iterations for burn-in.
tune	Number for iterations for tuning. The algorithm will be tuned to an acceptance rate between 0.3 and 0.6.
ab.ktrans	Mean and variance parameter for Gaussian prior on $\log(K^{trans})$ .
ab.kep	Mean and variance parameter for Gaussian prior on $\log(k_{ep})$ .
ab.vp	Hyper-prior parameters for the Beta prior on $v_p$ .
ab.gamma	...
ab.theta	...
ab.tauepsilon	Hyper-prior parameters for observation error Gamma prior.



samples	If TRUE output includes samples drawn from the posterior distribution for all parameters.
multicore	If TRUE algorithm is parallelized using <b>multicore</b> .
verbose	Logical variable (default = FALSE) that allows text-based feedback during execution of the function.
dic	If TRUE, the deviance information criterion (DIC) and effective number of parameters (pD) will be computed. If “samples = TRUE”, then samples of the DIC and pD will be given.
aif.model	...
aif.parameter	...
vp	...
...	Additional parameters to the function.

### Details

See Schmid *et al.* (2006) for details.

### Value

Parameter estimates and their standard errors are provided for the masked region of the multidimensional array. All multi-dimensional arrays are output in `nifti` format.

They include:

ktrans	Transfer rate from plasma to the extracellular, extravascular space (EES).
ktranserror	Error on $K^{trans}$ .
kep	Rate parameter for transport from the EES to plasma.
kepperror	Error on $k_{ep}$ .
ve	Fractional occupancy by EES (the ratio between ktrans and kep).
vperror	Error on $v_e$ .
vp	Fractional occupancy by plasma.
sigma2	The residual sum-of-squares from the model fit.
time	Acquisition times (for plotting purposes).
DIC	Deviance information criterion.
DIC.map	Contribution to DIC per voxel.
pD	Effective number of parameters.
pD.map	Contribution to pD per voxel.

Note, not all parameters are available under all models choices.

### Author(s)

Volker Schmid <volkerschmid@users.sourceforge.net>

## References

Schmid, V., Whitcher, B., Padhani, A.R., Taylor, N.J. and Yang, G.-Z. (2006) Bayesian methods for pharmacokinetic models in dynamic contrast-enhanced magnetic resonance imaging, *IEEE Transactions on Medical Imaging*, **25** (12), 1627-1636.

## See Also

[dcmri.lm](#), [dcmri.map](#), [dcmri.spline](#)

## Examples

```
data("buckley")
xi <- seq(5, 300, by=5)
img <- array(t(breast$data)[,xi], c(13,1,1,60))
mask <- array(TRUE, dim(img)[1:3])
time <- buckley$time.min[xi]

## Bayesian estimation with Fritz-Hansen default AIF
fit.bayes <- dcmri.bayes(img, time, mask, aif="fritz.hansen")

## Bayesian estimation with "orton.exp" function fit to Buckley's AIF
aif <- buckley$input[xi]
aifparams <- orton.exp.lm(time, aif)
aifparams$D <- 1
fit.bayes.aif <- dcmri.bayes(img, time, mask, model="orton.exp",
                             aif="user", user=aifparams)

plot(breast$ktrans, fit.bayes$ktrans, xlim=c(0,1), ylim=c(0,1),
      xlab=expression(paste("True ", K^{trans})),
      ylab=expression(paste("Estimated ", K^{trans}, " (Bayesian)")))
points(breast$ktrans, fit.bayes.aif$ktrans, pch=2)
abline(0, 1, lwd=2, col=2)
legend("right", c("extended/fritz.hansen", "orton.exp/user"), pch=1:2)
cbind(breast$ktrans, fit.bayes$ktrans[, ,1], fit.bayes.aif$ktrans[, ,1])

fit.lm <- dcmri.lm(img, time, mask, aif="fritz.hansen")
fit.lm.aif <- dcmri.lm(img, time, mask, model="orton.exp", aif="user",
                       user=aifparams)

plot(breast$ktrans, fit.bayes$ktrans, xlim=c(0,1), ylim=c(0,1),
      xlab=expression(paste("True ", K^{trans})),
      ylab=expression(paste("Estimated ", K^{trans})))
points(breast$ktrans, fit.bayes.aif$ktrans, pch=2)
points(breast$ktrans, fit.lm$ktrans, pch=3)
points(breast$ktrans, fit.lm.aif$ktrans, pch=4)
abline(0, 1, lwd=2, col=2)
legend("bottomright", c("Bayesian Estimation (fritz-hansen)",
                        "Bayesian Estimation (orton.exp)",
                        "Levenburg-Marquardt (weinmann/fritz.hansen)",
                        "Levenburg-Marquardt (orton.exp/user)"), pch=1:4)
```

dcmri.lm

*Pharmacokinetic Models for Dynamic Contrast-Enhanced MRI Data***Description**

Parameter estimation for single compartment models is performed using literature-based or user-specified arterial input functions. The Levenburg-Marquardt algorithm does the heavy lifting.

**Usage**

```
## S4 method for signature 'array'
dcmri.lm(conc, time, img.mask, model="extended", aif=NULL,
         control=minpack.lm::nls.lm.control(), user=NULL, guess=NULL,
         multicore=FALSE, verbose=FALSE, ...)
```

**Arguments**

conc	is a multidimensional (1D-4D) array of contrast agent concentrations. The last dimension is assumed to be temporal, while the previous dimensions are assumed to be spatial.
time	is a vector of acquisition times (in minutes) relative to injection of the contrast agent. Negative values should be used prior to the injection.
img.mask	is a (logical) multidimensional array that identifies the voxels to be analyzed. Has to have same dimension as conc minus temporal dimension.
model	is a character string that identifies the type of compartmental model to be used. Acceptable models include: <b>“weinmann”</b> Tofts & Kermode AIF convolved with single compartment model <b>“extended”</b> Weinmann model extended with additional vascular compartment (default) <b>“orton.exp”</b> Extended model using Orton’s exponential AIF <b>“orton.cos”</b> Extended model using Orton’s raised cosine AIF <b>“kety.orton.exp”</b> Kety model using Orton’s exponential AIF <b>“kety.orton.cos”</b> Kety model using Orton’s raised cosine AIF
aif	is a character string that identifies the parameters of the type of arterial input function (AIF) used with the above model. Acceptable values are: <ul style="list-style-type: none"> <li>• tofts.kermode(default) for the weinmann and extended models</li> <li>• fritz.hansen for the weinmann and extended models</li> <li>• “empirical” for the weinmann and extended models</li> <li>• orton.exp(default) for the orton.exp and kety.orton.exp model</li> <li>• orton.cos(default) for the orton.cos and kety.orton.cos model.</li> <li>• user for the orton.exp and orton.cos model.</li> </ul>

All AIF models set the parametric form and parameter values – except user, where a set of user-defined parameter values are allowed, and empirical, where a vector of values that fully characterize the empirical AIF.

control	is a list of parameters used by <code>nls.lm.control</code> that are set by default, but may be customized by the user.
user	is a list with the following parameters required: D, AB, muB, AG, muG.
guess	is a vector of starting values for kinetic parameter estimation. The vector must have length = 3 (with names <code>th0</code> , <code>th1</code> and <code>th3</code> ) when the extended Kety model is used with the vascular parameter and length = 2 (with names <code>th1</code> and <code>th3</code> ) otherwise.
multicore	is a logical variable (default = FALSE) that allows parallel processing via <b>multi-core</b> .
verbose	is a logical variable (default = FALSE) that allows text-based feedback during execution of the function.
...	Additional parameters to the function.

### Details

Compartmental models are the solution to the modified general rate equation (Kety 1951). The specific parametric models considered here include the basic Kety model

$$C_t(t) = K^{trans} [C_p(t) \otimes \exp(-k_{ep}t)],$$

where  $\otimes$  is the convolution operator, and the so-called extended Kety model

$$C_t(t) = v_p C_p(t) + K^{trans} [C_p(t) \otimes \exp(-k_{ep}t)].$$

The arterial input function must be either literature-based (with fixed parameters) or the exponential AIF from Orton *et al.* (2008) with user-defined parameters.

### Value

Parameter estimates and their standard errors are provided for the masked region of the multidimensional array. All multi-dimensional arrays are provided in `nifti` format.

They include:

ktrans	Transfer rate from plasma to the extracellular, extravascular space (EES).
kep	Rate parameter for transport from the EES to plasma.
ve	Fractional occupancy by EES (the ratio between $K^{trans}$ and $k_{ep}$ ).
vp	Fractional occupancy by plasma.
ktranserror	Standard error for $K^{trans}$ .
kepererror	Standard error for $k_{ep}$ .
vperror	Standard error for $v_p$ .

The residual sum-of-squares is also provided, along with the original acquisition times (for plotting purposes).

**Note**

WARNING: when using the empirical AIF, a linear interpolation is used to upsample the AIF to a one-second sampling rate. This allows one to utilize a computationally efficient numeric method to perform the convolution. If the empirical AIF is sampled faster than one Hertz, then the upsampling operation will become a downsampling operation. This should not have any serious effect on the parameter estimates, but caution should be exercised if very fast sampling rates are used to obtain an empirical AIF.

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>, Volker Schmid <volkerschmid@users.sourceforge.net>

**References**

- Ahearn, T.S., Staff, R.T., Redpath, T.W. and Semple, S.I.K. (2005) The use of the Levenburg-Marquardt curve-fitting algorithm in pharmacokinetic modelling of DCE-MRI data, *Physics in Medicine and Biology*, **50**, N85-N92.
- Fritz-Hansen, T., Rostrup, E., Larsson, H.B.W, Sondergaard, L., Ring, P. and Henriksen, O. (1993) Measurement of the arterial concentration of Gd-DTPA using MRI: A step toward quantitative perfusion imaging, *Magnetic Resonance in Medicine*, **36**, 225-231.
- Orton, M.R., Collins, D.J., Walker-Samuel, S., d'Arcy, J.A., Hawkes, D.J., Atkinson, D. and Leach, M.O. (2007) Bayesian estimation of pharmacokinetic parameters for DCE-MRI with a robust treatment of enhancement onset time, *Physics in Medicine and Biology* **52**, 2393-2408.
- Orton, M.R., d'Arcy, J.A., Walker-Samuel, S., Hawkes, D.J., Atkinson, D., Collins, D.J. and Leach, M.O. (2008) Computationally efficient vascular input function models for quantitative kinetic modelling using DCE-MRI, *Physics in Medicine and Biology* **53**, 1225-1239.
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- Tofts, P.S. and Kermode, A.G. (1984) Measurement of the blood-brain barrier permeability and leakage space using dynamic MR imaging. 1. Fundamental concepts, *Magnetic Resonance in Medicine*, **17**, 357-367.
- Weinmann, H.J., Laniado, M. and Mutzel, W. (1984) Pharmacokinetics of Gd-DTPA/dimeglumine after intravenous injection into healthy volunteers, *Physiological Chemistry and Physics and Medical NMR*, **16**, 167-172.

**See Also**

[dcmri.bayes](#), [dcmri.map](#), [dcmri.spline](#), [nls.lm](#)

**Examples**

```
data("buckley")

## Empirical arterial input function
img <- array(t(breast$data), c(13,1,1,301))
```

```

time <- buckley$time.min
mask <- array(TRUE, dim(img)[1:3])

## Estimate kinetic parameters directly from Buckley's empirical AIF
fit1 <- dcmri.lm(img, time, mask, model="weinmann", aif="empirical",
                user=buckley$input)
fit2 <- dcmri.lm(img, time, mask, model="extended", aif="empirical",
                user=buckley$input)

## Set up breast data for dcmri
xi <- seq(5, 300, by=3)
img <- array(t(breast$data)[,xi], c(13,1,1,length(xi)))
time <- buckley$time.min[xi]
input <- buckley$input[xi]

## Generate AIF params using the orton.exp function from Buckley's AIF
(aifparams <- orton.exp.lm(time, input))
fit3 <- dcmri.lm(img, time, mask, model="orton.exp", aif="user",
                user=aifparams)

## Scatterplot comparing true and estimated Ktrans values
plot(breast$ktrans, fit1$ktrans, xlim=c(0,0.75), ylim=c(0,0.75),
     xlab=expression(paste("True ", K^{trans})),
     ylab=expression(paste("Estimated ", K^{trans})))
points(breast$ktrans, fit2$ktrans, pch=2)
points(breast$ktrans, fit3$ktrans, pch=3)
abline(0, 1, lwd=1.5, col=2)
legend("bottomright", c("weinmann/empirical", "extended/empirical",
                       "orton.exp/user"), pch=1:3)
cbind(breast$ktrans, fit1$ktrans[,1], fit2$ktrans[,1], fit3$ktrans[,1])

## Scatterplot comparing true and estimated Ktrans values
plot(breast$vp, fit1$vp, type="n", xlim=c(0,0.15), ylim=c(0,0.15),
     xlab=expression(paste("True ", v[p])),
     ylab=expression(paste("Estimated ", v[p])))
points(breast$vp, fit2$vp, pch=2)
points(breast$vp, fit3$vp, pch=3)
abline(0, 1, lwd=1.5, col=2)
legend("bottomright", c("extended/empirical", "orton.exp/user"), pch=2:3)
cbind(breast$vp, fit2$vp[,1], fit3$vp[,1])

```

---

dcmri.map

*Pharmacokinetic Modeling of Dynamic Contrast-Enhanced MRI Data*


---

## Description

Maximum-a-posteriori (MAP) estimation for single compartment models is performed using literature-based or user-specified arterial input functions.

**Usage**

```
## S4 method for signature 'array'
dcmri.map(conc, time, img.mask, model="extended", aif=NULL,
          user=NULL, ab.ktrans=c(0,1), ab.kep=ab.ktrans,
          ab.vp=c(1,19), ab.tauepsilon=c(1,1/1000), maxit=5000,
          samples=FALSE, multicore=FALSE, verbose=FALSE, ...)
```

**Arguments**

conc	Matrix or array of concentration time series (last dimension must be time).
time	Time in minutes.
img.mask	Mask matrix or array. Voxels with mask=0 will be excluded.
model	is a character string that identifies the type of compartmental model to be used. Acceptable models include: <ul style="list-style-type: none"> <li>• “weinmann”Tofts &amp; Kermode AIF convolved with single compartment model</li> <li>• “extended”Weinmann model extended with additional vascular compartment (default)</li> <li>• “orton.exp”Extended model using Orton’s exponential AIF</li> <li>• “kety.orton.exp”Kety model using Orton’s exponential AIF</li> <li>• “orton.cos”Extended model using Orton’s raised cosine AIF</li> <li>• “kety.orton.cos”Kety model using Orton’s raised cosine AIF</li> </ul>
aif	is a character string that identifies the parameters of the type of arterial input function (AIF) used with the above model. Acceptable values are: tofts.kermode (default) or fritz.hansen for the weinmann and extended models; orton.exp (default) or user for the orton.exp model and orton.exp model; user for the orton.cos model and orton.cos model.
user	Vector of AIF parameters. For Tofts and Kermode: $a_1, m_1, a_2, m_2$ ; for Orton <i>et al.</i> : $A_b, \mu_b, A_g, \mu_g$ .
ab.ktrans	Mean and variance parameter for Gaussian prior on $\log(K^{trans})$ .
ab.kep	Mean and variance parameter for Gaussian prior on $\log(k_{ep})$ .
ab.vp	Hyper-prior parameters for the Beta prior on $v_p$ .
ab.tauepsilon	Hyper-prior parameters for observation error Gamma prior.
maxit	The maximum number of iterations for the optimization procedure.
samples	If TRUE output includes samples drawn from the posterior distribution for all parameters.
multicore	If TRUE algorithm is parallelized using <b>multicore</b> .
verbose	Logical variable (default = FALSE) that allows text-based feedback during execution of the function.
...	Additional parameters to the function.

**Details**

Implements *maximum a posteriori* (MAP) estimation for the Bayesian model in Schmid *et al.* (2006).

**Value**

Parameter estimates and their standard errors are provided for the masked region of the multidimensional array. The multi-dimensional arrays are provided in `nifti` format.

They include:

<code>ktrans</code>	Transfer rate from plasma to the extracellular, extravascular space (EES).
<code>kep</code>	Rate parameter for transport from the EES to plasma.
<code>ve</code>	Fractional occupancy by EES (the ratio between <code>ktrans</code> and <code>kep</code> ).
<code>vp</code>	Fractional occupancy by plasma.
<code>sigma2</code>	The residual sum-of-squares from the model fit.
<code>time</code>	Acquisition times (for plotting purposes).

Note, not all parameters are available under all models choices.

**Author(s)**

Volker Schmid <volkerschmid@users.sourceforge.net>

**References**

Schmid, V., Whitcher, B., Padhani, A.R., Taylor, N.J. and Yang, G.-Z. (2006) Bayesian methods for pharmacokinetic models in dynamic contrast-enhanced magnetic resonance imaging, *IEEE Transactions on Medical Imaging*, **25** (12), 1627-1636.

**See Also**

[dcmri.lm](#), [dcmri.bayes](#)

**Examples**

```
data("buckley")
xi <- seq(5, 300, by=5)
img <- array(t(breast$data)[,xi], c(13,1,1,60))
mask <- array(TRUE, dim(img)[1:3])
time <- buckley$time.min[xi]

## MAP estimation with extended Kety model and Fritz-Hansen default AIF
fit.map.vp <- dcmri.map(img, time, mask, aif="fritz.hansen")
## Nonlinear regression with extended Kety model and Fritz-Hansen default AIF
fit.lm.vp <- dcmri.lm(img, time, mask, aif="fritz.hansen")

plot(breast$ktrans, fit.map.vp$ktrans, xlim=c(0,1), ylim=c(0,1),
      xlab=expression(paste("True ", K^{trans})),
      ylab=expression(paste("Estimated ", K^{trans})))
points(breast$ktrans, fit.lm.vp$ktrans, pch=3)
abline(0, 1, lwd=2, col=2)
legend("bottomright", c("MAP Estimation (fritz.hansen)",
                        "Levenburg-Marquardt (fritz.hansen)"), pch=c(1,3))
```



```
## MAP estimation with Kety model and Fritz-Hansen default AIF
fit.map <- dcmri.map(img, time, mask, model="weinmann", aif="fritz.hansen")
## Nonlinear regression with Kety model and Fritz-Hansen default AIF
fit.lm <- dcmri.lm(img, time, mask, model="weinmann", aif="fritz.hansen")

cbind(breast$kep, fit.lm$kep[, ,1], fit.lm.vp$kep[, ,1], fit.map$kep[, ,1],
      fit.map.vp$kep[, ,1])
cbind(breast$ktrans, fit.lm$ktrans[, ,1], fit.lm.vp$ktrans[, ,1],
      fit.map$ktrans[, ,1], fit.map.vp$ktrans[, ,1])
```

---

dcmri.spline

*Bayesian P-Splines for Dynamic Contrast-Enhanced MRI Data*


---

## Description

Quantitative analysis of DCE-MRI typically involves the convolution of an arterial input function (AIF) with a nonlinear pharmacokinetic model of the contrast agent concentration. This function takes a semi-parametric penalized spline smoothing approach, with which the AIF is convolved with a set of B-splines to produce a design matrix using locally adaptive smoothing parameters based on Bayesian penalized spline models (P-splines).

## Usage

```
## S4 method for signature 'array'
dcmri.spline(conc, time, img.mask, time.input=time,
             model="weinmann", aif="tofts.kermode", user=NULL,
             aif.observed=NULL, nriters=500, thin=5,
             burnin=100, ab.hyper=c(1e-5,1e-5),
             ab.tauepsilon=c(1,1/1000), k=4, p=25, rw=2,
             knots=NULL, nlr=FALSE, t0.compute=FALSE,
             samples=FALSE, multicore=FALSE, verbose=FALSE,
             response=FALSE, fitted=FALSE,
             ...)
dcmri.spline.single(conc, time, D, time.input, p, rw, knots, k,
                   A, t0.compute=FALSE, nlr=FALSE, nriters=500,
                   thin=5, burnin=100, ab.hyper=c(1e-5,1e-5),
                   ab.tauepsilon=c(1,1/1000), silent=0,
                   multicore=FALSE, model=NULL,
                   model.func=NULL, model.guess=NULL,
                   samples=FALSE, B=NULL)
```

## Arguments

conc	Matrix or array of concentration time series (last dimension must be time).
time	Time in minutes.
img.mask	Mask matrix or array. Voxels with mask = 0 will be excluded.
time.input	Time in minutes for observed arterial input function (default = 'time').

aif	is a character string that identifies the parameters of the arterial input function. Acceptable values are: tofts.kermode, fritz.hansen or observed. If observed you must provide the observed concentrations in aif.observed.
user	...
aif.observed	is the user-defined vector of arterial concentrations observed at time.input (only for 'aif'=observed).
silent	...
multicore	(logical) use the <b>multicore</b> package.
verbose	(logical) allows text-based feedback during execution of the function (default = FALSE).
samples	If TRUE output includes samples drawn from the posterior distribution for all parameters.
model.func	...
model.guess	...
nlr	If TRUE, a response model is fitted to the estimated response function.
model	Only if nlr = TRUE Response model fitted to the estimated response function. Acceptable values include: "AATH" or "weinmann" (default).
ab.hyper	Hyper priors for adaptive smoothness parameter
ab.tauepsilon	Hyper-prior parameters for observation error Gamma prior.
p	Number of knots of B-Spline basis.
t0.compute	If TRUE, the onset time will be estimated from response function.
k	Order of B-Splines.
knots	Vector of knots. Use this if you need unequally spaced knots.
rw	Order of random walk prior. Acceptable values are 1 and 2.
nriters	Total number of iterations.
thin	Thining factor.
burnin	Number of iterations for burn-in.
response	If TRUE, the response functions per voxel are returned.
fitted	If TRUE, then fitted time curved per voxel are returned.
A	...
B	...
D	...
...	...

## Details

See Schmid *et al.* (2009) for more details.

## Value

The maximum of the response function  $F_p$  for the masked region is provided by default. Where appropriate, response functions, fitted functions, and parameter estimates (along with their standard errors) are provided. All multi-dimensional arrays are provided in `nifti` format.

**Author(s)**

Volker Schmid <<volkerschmid@users.sourceforge.net>>

**References**

Schmid, V., Whitcher, B., Padhani, A.R. and G.-Z. Yang (2009) A semi-parametric technique for the quantitative analysis of dynamic contrast-enhanced MR images based on Bayesian P-splines, *IEEE Transactions on Medical Imaging*, **28** (6), 789-798.

**See Also**

[dcmri.bayes](#), [dcmri.lm](#), [dcmri.map](#)

**Examples**

```
data("buckley")
xi <- seq(5, 300, by=5)
img <- array(t(breast$data)[,xi], c(13,1,1,60))
mask <- array(TRUE, dim(img)[1:3])
time <- buckley$time.min[xi]

## Generate AIF params using the orton.exp function from Buckley's AIF
aif <- buckley$input[xi]

fit.spline <- dcmri.spline(img, time, mask, aif="fritz.hansen",
                          nriters=250, nlr=TRUE)
fit.spline.aif <- dcmri.spline(img, time, mask, aif="observed",
                              aif.observed=aif, nriters=250,
                              nlr=TRUE)

plot(breast$ktrans, fit.spline$ktrans, xlim=c(0,1), ylim=c(0,1),
     xlab=expression(paste("True ", K^{trans})),
     ylab=expression(paste("Estimated ", K^{trans})))
points(breast$ktrans, fit.spline.aif$ktrans, pch=2)
abline(0, 1, lwd=1.5, col="red")
legend("right", c("fritz.hansen", "observed"), pch=1:2)

cbind(breast$ktrans, fit.spline$ktrans[, ,1], fit.spline.aif$ktrans[, ,1])
```

---

expConv

*Convolution*

---

**Description**

...

**Usage**

```
expConv(input, k1, k2)
```

**Arguments**

input            ...  
k1                ...  
k2                ...

**Details**

...

**Value**

...

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>

---

find.center

*Find the Center of a Binary Mask*

---

**Description**

The center of a binary mask is determined.

**Usage**

```
find.center(M)
```

**Arguments**

M                    is a binary mask (multidimensional array of logical values).

**Details**

This method most likely only works with convex three-dimensional shapes (e.g., a hyper-rectangle). Further testing is required to know the limits of the current implementation.

**Value**

A vector of values the same length as the input array.

**Author(s)**

Brandon Whitcher

**See Also**

[ftm](#)

## Examples

```
M <- array(FALSE, rep(10,3))
M[6:10,6:10,6:10] <- TRUE
Mc <- find.center(M)
print(Mc)
```

---

ftm

*Fast Template Matching via Cross-Correlation*

---

## Description

Motion correction and/or co-registration of three-dimensional arrays (medical imaging data) are performed by applying a user-defined mask of voxels. Normalized cross-correlations (in 3D) are computed using the FFT.

## Usage

```
## S4 method for signature 'array'
ftm(input, ...)
```

## Arguments

input	is a four-dimensional array of signal intensities.
...	Additional variables passed to the plot function.

## Details

An extremely basic method of motion correction/co-registration is implemented by estimating “local” cross-correlations based on a binary mask that is a subset of the original three-dimensional volume. All convolutions are performed via the FFT ([fft](#)) and repetitive calculations are minimized where possible.

Only whole-voxel translations are considered. This does not begin to capture the true effects of motion in soft tissue, but we assume that the object of interest (e.g., tumor) is a fairly rigid structure. Potential extensions include rigid-body, affine and nonlinear registration techniques along with interpolation schemes in order to capture intra-voxel manipulations of the data.

## Value

A list of objects are returned:

out	Motion-corrected version of the four-dimensional array.
offset	Translations (in 3D) for each volume in the 4D array.
t.center	Estimated center of the binary mask.

## Author(s)

Brandon Whitcher <<bjw34032@users.sourceforge.net>>

**References**

Lewis, J.P. (2003) Fast normalized cross-correlation.  
[www.idiom.com/~zilla/](http://www.idiom.com/~zilla/)

**See Also**

[conv.fft](#), [find.center](#), [shift3D](#)

---

 kineticModel

*Pharmacokinetic Models*


---

**Description**

Kinetic curves from single compartment models are computed from kinetic parameters.

**Usage**

```
kineticModel(time, par, model="extended", aif="fritz.hansen")
```

**Arguments**

time	is a vector of acquisition times (in minutes).
par	is a list of kinetic parameters; e.g., <code>list("ktrans"=0.5, "kep"=1)</code> .
model	is a character string that identifies the type of compartmental model to be used. Acceptable models include: "weinmann" Tofts & Kermode AIF convolved with single compartment model "extended" (default) Weinmann model extended with additional vascular compartment, ...
aif	is a character string that identifies the type of arterial input function (AIF) to be used. Acceptable AIF models include: <code>tofts.kermode</code> , <code>fritz.hansen</code>

**Details**

Compartmental models are the solution to the modified general rate equation (Kety 1951). The specific parametric models considered here include the basic Kety model

$$C_t(t) = K^{trans} [C_p(t) \otimes \exp(-k_{ep}t)],$$

where  $\otimes$  is the convolution operator, and the so-called extended Kety model

$$C_t(t) = v_p C_p(t) + K^{trans} [C_p(t) \otimes \exp(-k_{ep}t)].$$

The arterial input function must be literature-based (with fixed parameters).

**Value**

Computed pharmacokinetic curve.

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net> and Volker Schmid <volkerschmid@users.sourceforge.net>

**References**

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Tofts, P.S., Brix, G, Buckley, D.L., Evelhoch, J.L., Henderson, E., Knopp, M.V., Larsson, H.B.W., Lee, T.-Y., Mayr, N.A., Parker, G.J.M., Port, R.E., Taylor, J. and Weiskoff, R. (1999) Estimating kinetic parameters from dynamic contrast-enhanced  $T_1$ -weighted MRI of a diffusable tracer: Standardized quantities and symbols, *Journal of Magnetic Resonance*, **10**, 223-232.

Tofts, P.S. and Kermode, A.G. (1984) Measurement of the blood-brain barrier permeability and leakage space using dynamic MR imaging. 1. Fundamental concepts, *Magnetic Resonance in Medicine*, **17**, 357-367.

Weinmann, H.J., Laniado, M. and Mutzel, W. (1984) Pharmacokinetics of Gd-DTPA/dimeglumine after intravenous injection into healthy volunteers, *Physiological Chemistry and Physics and Medical NMR*, **16**, 167-172.

**See Also**

[dcmri.lm](#), [dcmri.bayes](#), [dcmri.spline](#)

**Examples**

```
data("buckley")
xi <- seq(5, 300, by=5)
img <- array(t(breast$data)[,xi], c(13,1,1,60))
mask <- array(TRUE, dim(img)[1:3])
time <- buckley$time.min[xi]

fit.lm <- dcmri.lm(img, time, mask, aif="fritz.hansen")
par.lm <- c("vp"=fit.lm$vp[3], "ktrans"=fit.lm$ktrans[3], "kep"=fit.lm$kep[3])
curve.lm <- kineticModel(time, par.lm)
plot(time, img[3,1,1,], xlab="time", ylab="contrast agent concentration")
lines(time, curve.lm, lwd=2, col=2)

fit.bayes <- dcmri.bayes(img, time, mask, aif="fritz.hansen")
par.bayes <- c("vp"=fit.bayes$vp[3], "ktrans"=fit.bayes$ktrans[3],
              "kep"=fit.bayes$kep[3])
curve.bayes <- kineticModel(time, par.bayes)
lines(time, curve.bayes, lwd=2, col=4)
legend("bottomright", c("Levenburg-Marquardt (extended/fritz.hansen)",
                        "Bayesian Estimation (extended/fritz-hansen)"),
       lwd=2, col=c(2,4))
cbind(time, img[3,,], curve.lm, curve.bayes)[20:30,]
```

rCBV

*Regional Cerebral Blood Volume***Description**

...

**Usage**

```
rCBV(Ct, Ca, time, Hf=1, rho=1)
## S4 method for signature 'array'
rCBV.fast(signal, mask, aif, time, multicore=FALSE, verbose=FALSE)
```

**Arguments**

Ct	...
Ca	...
time	is the vector of acquisition times associated with the dynamic data.
Hf	...
rho	...
signal	is a multidimensional array of signal intensities (or concentrations). The last dimension is assumed to be a function of the acquisition times, while the previous dimensions are assumed to be spatial.
mask	is a (logical) multidimensional array that identifies the voxels to be analyzed.
aif	Arterial Input Function.
multicore	is a logical variable (default = FALSE) that allows parallel processing via <b>multicore</b> .
verbose	is a logical variable (default = FALSE) that allows text-based feedback during execution of the function.

**Details**

...

**Value**

A nifti object containing the estimates of regional cerebral blood volume (rCBV).

**Author(s)**

Brandon Whitcher <bjw34032@users.sourceforge.net>



Relaxivity

*Estimate Intrinsic Tissue Relaxivity***Description**

Estimation of the intrinsic tissue relaxivity is achieved through nonlinear optimization and the dynamic signal intensities are converted into contrast agent concentration.

**Usage**

```
R10.lm(signal, alpha, TR, guess, control=minpack.lm::nls.lm.control())
E10.lm(signal, alpha, guess, control=minpack.lm::nls.lm.control())
## S4 method for signature 'array'
R1.fast(flip, flip.mask, fangles, TR,
        control=minpack.lm::nls.lm.control(), multicore=FALSE,
        verbose=FALSE)
## S4 method for signature 'array'
CA.fast(dynamic, dyn.mask, dangle, flip, fangles, TR, r1=4,
        control=minpack.lm::nls.lm.control(maxiter=200), multicore=FALSE,
        verbose=FALSE)
## S4 method for signature 'array'
CA.fast2(dynamic, dyn.mask, dangle, flip, fangles, TR, r1=4,
        verbose=FALSE)
```

**Arguments**

signal	is the vector of signal intensities as a function of flip angles.
alpha	is the vector of flip angles (in degrees).
TR	is the relaxation time (in seconds) used in the acquisition of the MRI data.
guess	is the vector of initial values for the parameters of interest: $m_0$ and $R_{10}$ .
control	An optional list of control settings for <code>nls.lm</code> . See <code>nls.lm.control</code> for the names of the settable control values and their effect.
dynamic	a multidimensional array of contrast agent concentrations. The last dimension is assumed to be temporal, while the previous dimensions are assumed to be spatial.
flip.mask, dyn.mask	is a (logical) multidimensional array that identifies the voxels to be analyzed.
dangle	is the flip angle used to acquire the dynamic MRI data.
flip	a multidimensional array of contrast agent concentrations. The last dimension is assumed to be a function of the flip angles, while the previous dimensions are assumed to be spatial.
fangles	is the vector of flip angles (in degrees).
r1	is the spin-lattice relaxivity constant (default = 4.39 for 1.5T). For 3T data it may be necessary to adjust this value.

multicore	is a logical variable (default = FALSE) that allows parallel processing via <b>multicore</b> .
verbose	is a logical variable (default = FALSE) that allows text-based feedback during execution of the function.

### Details

The `E10.lm` and `R10.lm` functions estimate parameters for a vector of observed MR signal intensities, as a function of flip angle, using the following relationship

$$S(\alpha) = m_0 \frac{\sin(\alpha) (1 - \exp -\text{TR}/T_1)}{(1 - \cos(\alpha) \exp -\text{TR}/T_1)}.$$

The only difference between the two functions is exactly what is being estimated in the nonlinear least squares formulation. They both require the function `nls.lm` that uses the Levenberg-Marquardt algorithm.

The `CA.fast` function calls on `R1.fast` to rearrange the assumed multidimensional (2D or 3D) structure of the multiple flip-angle data into a single matrix to take advantage of internal R functions instead of loops when calling `E10.lm`. Conversion of the dynamic signal intensities to contrast agent concentration is performed via

$$[Gd] = \frac{1}{r_1} \left( \frac{1}{T_1} - \frac{1}{T_{10}} \right).$$

The `CA2.fast` function assumes only two flip angles have been acquired and uses an approximation to the nonlinear relationship between signal intensity and flip angle enable to conversion from signal intensity to contrast agent concentration.

### Value

A list structure is produced with (all or some of the) parameter estimates

<code>M0</code>	Scaling factor between signal intensity and $T_1$ .
<code>R10</code>	Pre-injection tissue relaxation rate (3D array); $R1_0 = 1/T1_0$ .
<code>R1t</code>	Time-varying tissue relaxation rate (4D array); $R1(t) = 1/T1(t)$ .
<code>conc</code>	Contrast agent concentration (4D array).

and information about the convergence of the nonlinear optimization routine.

### Note

The longitudinal relaxivity is set, by default, to  $r_1 = 4(mM \cdot s)^{-1}$  which is a reasonable value for gadolinium contrast agents at 1.5 Tesla. Double-check the scanning procedure manual to ensure the correct value is used.

### Author(s)

Brandon Whitcher <bjw34032@users.sourceforge.net>

## References

- Buxton, R.B. (2002) *Introduction to Functional Magnetic Resonance Imaging: Principles & Techniques*, Cambridge University Press: Cambridge, UK.
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## See Also

[dcmri.lm](#), [nls.lm](#)

## Examples

```
## Parameters for simulated data
S0 <- 100
TR <- 5 / 1000          # seconds
T1 <- 1.5              # seconds
alpha <- seq(2, 24, by=2) # degrees

## Signal intensities for spoiled gradient echo image
gre <- function(S0, TR, T1, alpha) {
  theta <- alpha * pi/180 # radians
  S0 * (1 - exp(-TR/T1)) * sin(theta) / (1 - cos(theta) * exp(-TR/T1))
}
set.seed(1234)
signal <- array(gre(S0, TR, T1, alpha) + rnorm(length(alpha), sd=.15),
               c(rep(1,3), length(alpha)))
out <- R1.fast(signal, array(TRUE, rep(1,3)), alpha, TR)
unlist(out)
plot(alpha, signal, xlab="Flip angle", ylab="Signal intensity")
lines(alpha, gre(S0, TR, T1, alpha), lwd=2, col=1)
lines(alpha, gre(out$M0, TR, 1/out$R10, alpha), lwd=2, col=2)
legend("topright", c("True", "Estimated"), lwd=2, col=1:2)
```

---

Seed Growing for a 4D Array

*Seed Growing for a 4D Array*

---

## Description

Seed growing algorithm to find voxels in a three-dimensional array according to their correlation to a seed voxel. The correlation is measured according to the fourth dimension of the array.

**Usage**

```
extract.aif(img, x, y, z, thresh = 0.9)
```

**Arguments**

img	is the four-dimensional array of medical imaging data.
x,y,z	are the coordinates of the seed voxel.
thresh	is the minimum correlation for inclusion in the region.

**Details**

Correlation coefficients are computed for every voxel in the input array. A recursive algorithm is then used to grow the region of interest (ROI) from the seed voxel in three dimensions. All adjacent voxels, where the correlation exceeds the threshold, are included.

**Value**

coord	is a matrix of the three-dimensional coordinates $(x, y, z)$ for all voxels found by the algorithm.
conc	is a matrix whose rows correspond to the voxels found by the algorithm and whose columns are the fourth dimension from the input array (e.g., contrast agent concentration time curve).
mask	is an array of boolean values, where only voxels included by the algorithm are given a value greater than zero.
cor	is an array that mimics the mask, but contains the estimated correlation coefficients for all voxels included by the algorithm.

**Author(s)**

Volker Schmid <<volker.schmid@users.sourceforge.net>>

---

 shift3D

---

*Shift a 3D Array in One Dimension*


---

**Description**

One axis of the three-dimensional array is translated by an integer amount. This is useful when applying convolution operators in the Fourier domain.

**Usage**

```
shift3D(A, s, type, fill=0)
```

**Arguments**

A	is a three-dimensional array.
s	is the integer number of translation steps.
type	is a character string using anatomical coordinates assuming a transverse acquisition scheme (“LR” = left-right = x-axis, “AP” = anterior-posterior = y-axis, “SI” = superior-inferior = z-axis).
fill	is the quantity used to fill gaps induced by the translations (circular boundary conditions are NOT used).

**Value**

A three-dimensional array is returned, the same dimension as the original array, with one dimension translated.

**Author(s)**

Brandon Whitcher

**See Also**

[conv.fft](#)

**Examples**

```
cube <- array(0, rep(20,3))
cube[9:12,9:12,9:12] <- 1
cube.shift <- shift3D(cube, 5, type="AP")
par(mfrow=c(1,2), mar=rep(0.5,4))
image(cube[, ,10], xlab="", ylab="", axes=FALSE)
image(cube.shift[, ,10], xlab="", ylab="", axes=FALSE)
```

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